

Registration using Dynamic Data

-- Data acquisition and analysis of dynamic data

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Outline

- 1 Introduction
- 2 Previous work
- 3 Overview of the planned work
- 4 Methodology: Data acquisition and analysis of dynamic data
- 5 Results
- 6 Conclusion

Registration?

- How to:
 - Optimally align two shapes in arbitrary configurations?

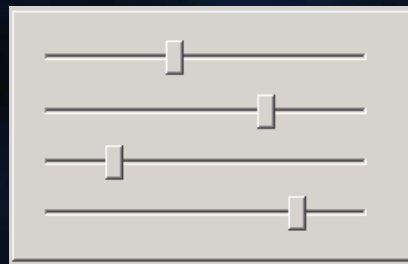
- Central problem in:
 - Image processing
 - Shape acquisition
 - Modeling

- Used to:
 - Compare
 - Integrate data
 - ✓ different measurement devices, viewpoints, times of measurement, ...
 - ✓ different subjects

Registration?

- Extrinsic vs. intrinsic
- 2D vs. 3D
- Rigid vs. non-rigid
- Inter-subject vs. intra-subject
- Image vs. surface, boundary vs. volume

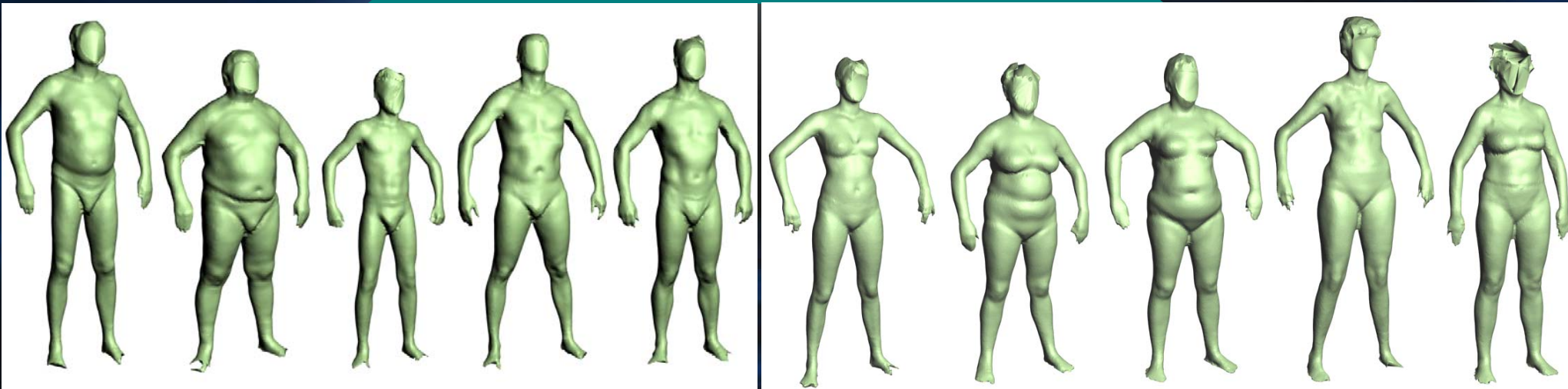
Example: 3D intra-subject surface registration



Body Modeler

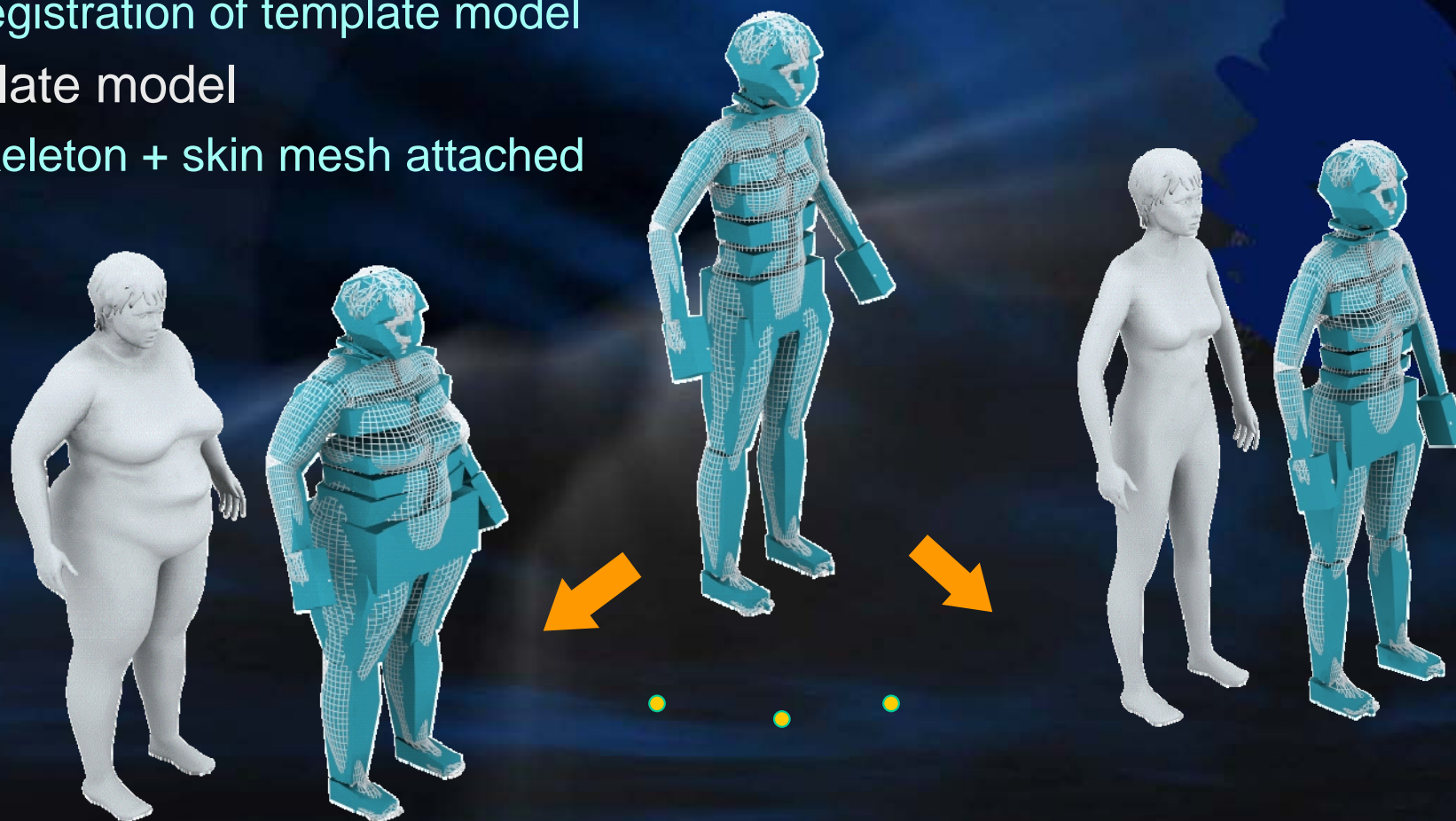


- Possible shape space
- Statistical tendencies



Example: 3D intra-subject surface registration

- Correspondence finding
 - Registration of template model
- Template model
 - Skeleton + skin mesh attached



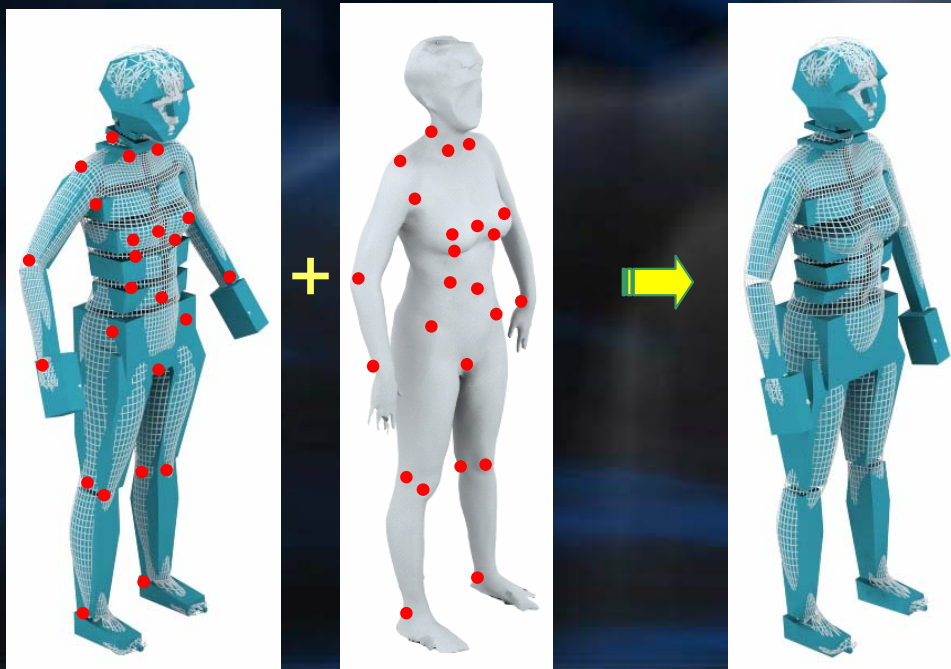
Example: 3D intra-subject surface registration

➤ Feature based approach

- to measure the fitting accuracy
- to guide the conformation

➤ 2 steps

- Joint transformation
- Vertex displacement



Registration of the template: problem formulation

- Joint transformation: Find \mathbf{x} such that $E(\mathbf{x})$ is minimized, where

$$\mathbf{x} = ([t_{x1}, t_{y1}, t_{z1}, \theta_{x1}, \theta_{y1}, \theta_{z1}, s_{x1}, s_{y1}, s_{z1}], \theta_{x2}, \dots, s_{xn}),$$

translation, rotation, and scale of root joint

$$E(\mathbf{x}) = \sum |P_i(\mathbf{x}) - P'_i|.$$

Distance between corresponding feature points

- Vertex displacement: Find vertex displacement \mathbf{d} that minimizes $E(\mathbf{d})$:

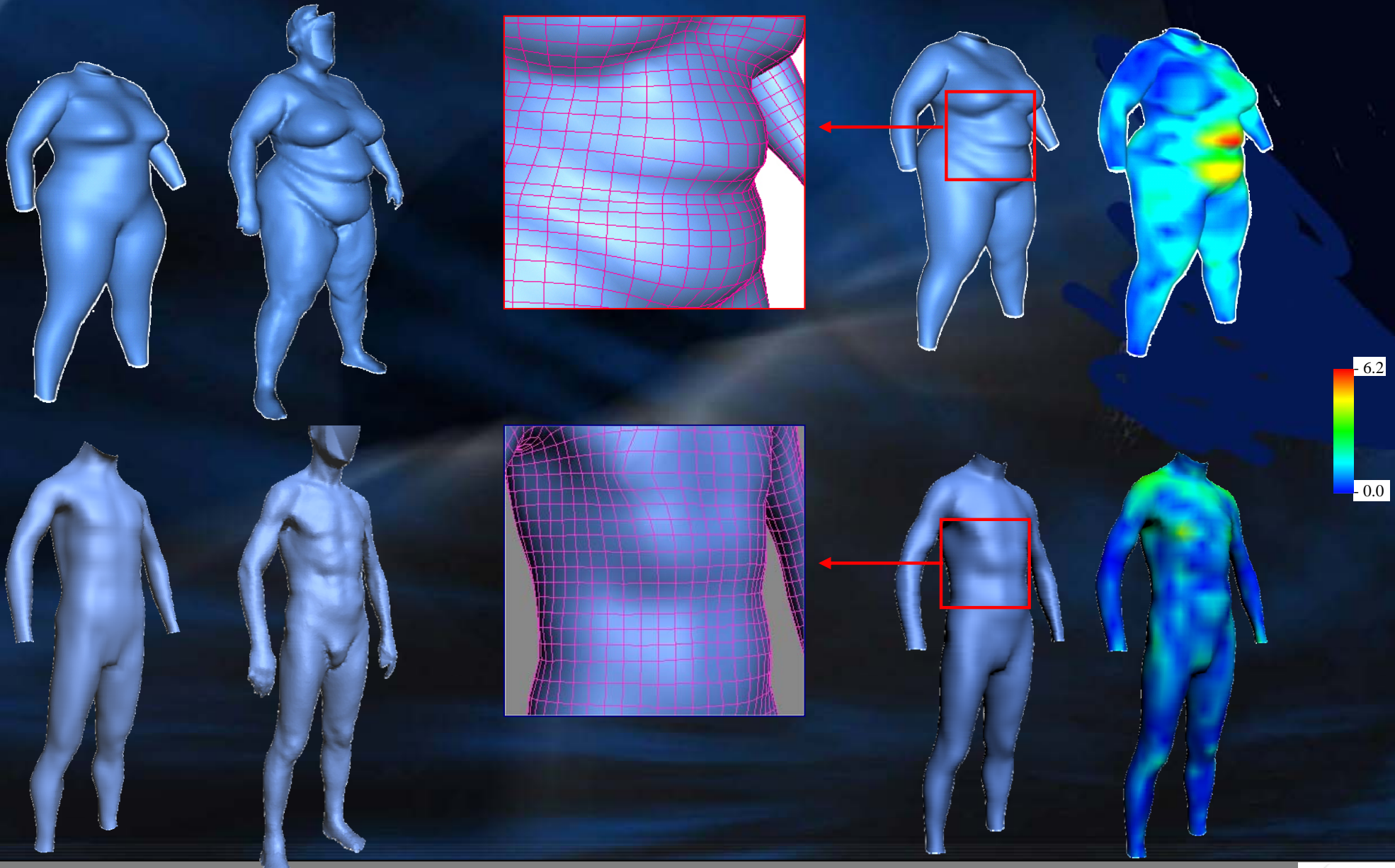
$$E(\mathbf{d}) = \alpha E_p(\mathbf{d}) + \beta E_s(\mathbf{d}) + \gamma E_d(\mathbf{d}).$$

Feature point
distance

Distortion
energy

Surface
distance

Registration of the template: results



Summary of registration in medical imaging

- Landmark based
 - Anatomical
 - geometrical
- Segmentation based
 - Rigid
 - Deformable model
- Voxel property based
 - Reduction to scalars/vectors (moments, principal axes)
 - Using full image content

Previous methods do not consider dynamic, time-varying features, despite their increasing clinical relevance!!

Overview

0. Motion data acquisition

- Movement data in temporal correspondence

1. Analysis of dynamic data

- Extraction of dynamic features

2. Registration using dynamic data

- Correspondence computation among dynamic features
- Transformation

3. Statistical atlas construction

- Dimension reduction
- Joint probabilistic map

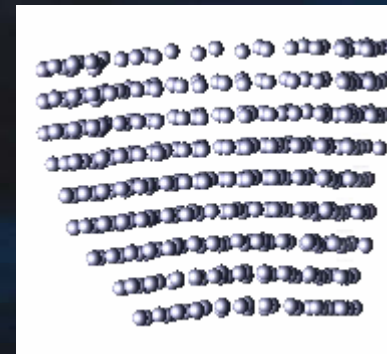
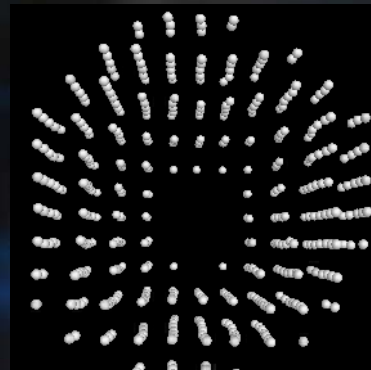
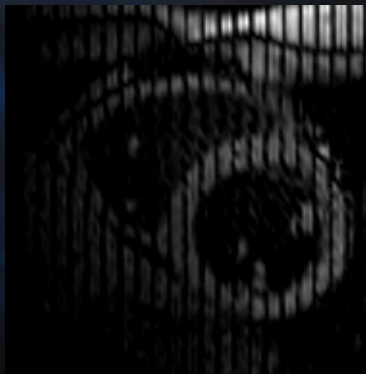
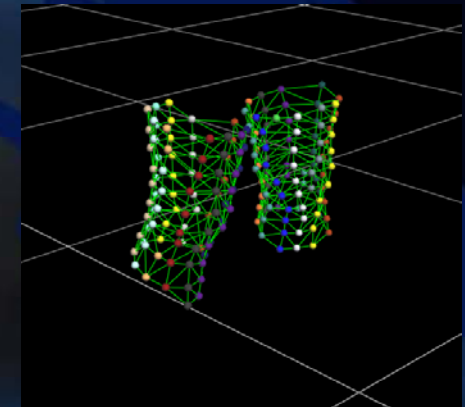
- Compact mathematical representation of the current shape and its motion behavior
- Incorporate registration variations (due to anatomical identity and due to movement)

4. Revision of registration

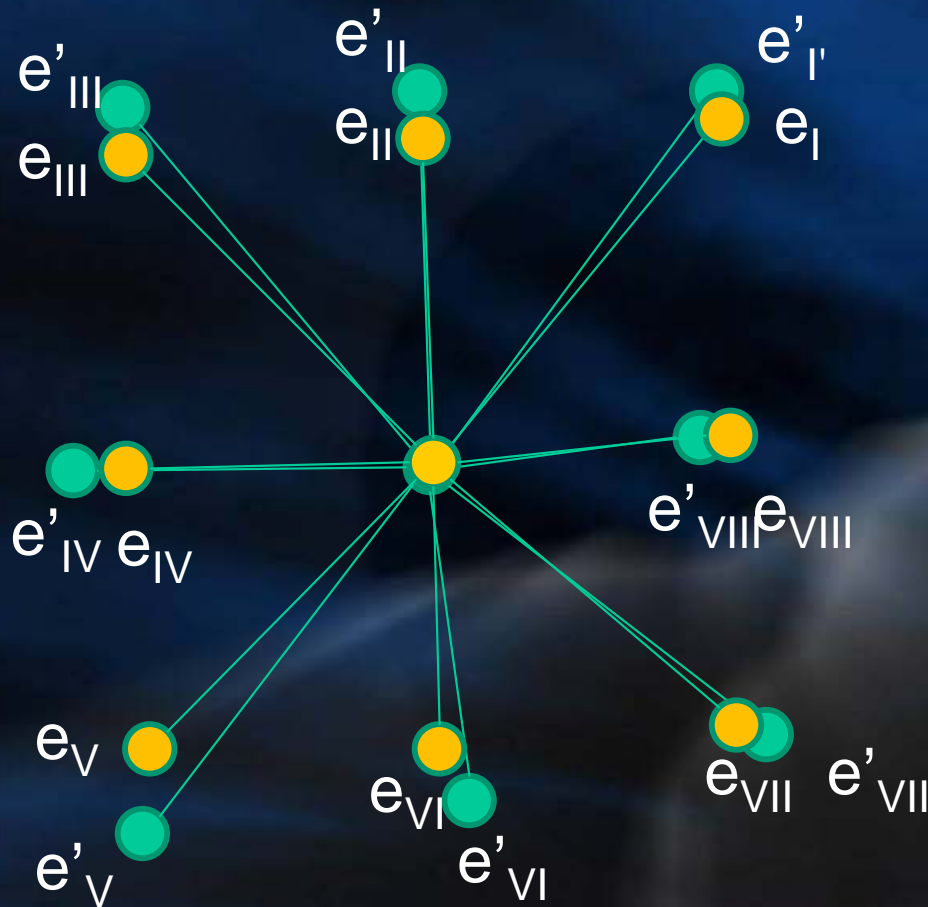
- Statistical atlas based registration

Motion data acquisition

- 3D scanner
 - With color markers
- Optical motion capture device
 - High frequency
- Tagged MRI
 - Temporal correspondence



Analysis of deforming surface



$$\varepsilon_I = \frac{e'_I - e_I}{e_I}$$

▪

▪

▪

$$\varepsilon_{VIII} = \frac{e'_{VIII} - e_{VIII}}{e_{VIII}}$$

➤ Adopt virtual strain gages and perform local strain analysis!!

Strain gage

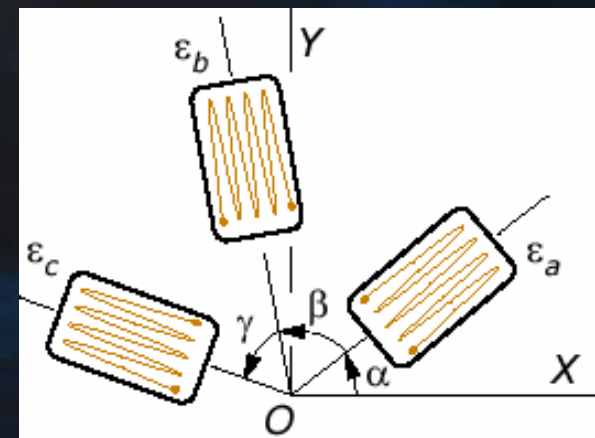
- Used to measure the strain of an object
- Linear strain gage
 - Strain along one direction
- Rosette strain gage
 - To determine the three independent components of plane strain, three linearly independent strain measures are needed



$$\varepsilon_a = \frac{\varepsilon_X + \varepsilon_Y}{2} + \frac{\varepsilon_X - \varepsilon_Y}{2} \cos 2\alpha + \gamma_{XY} \sin 2\alpha$$

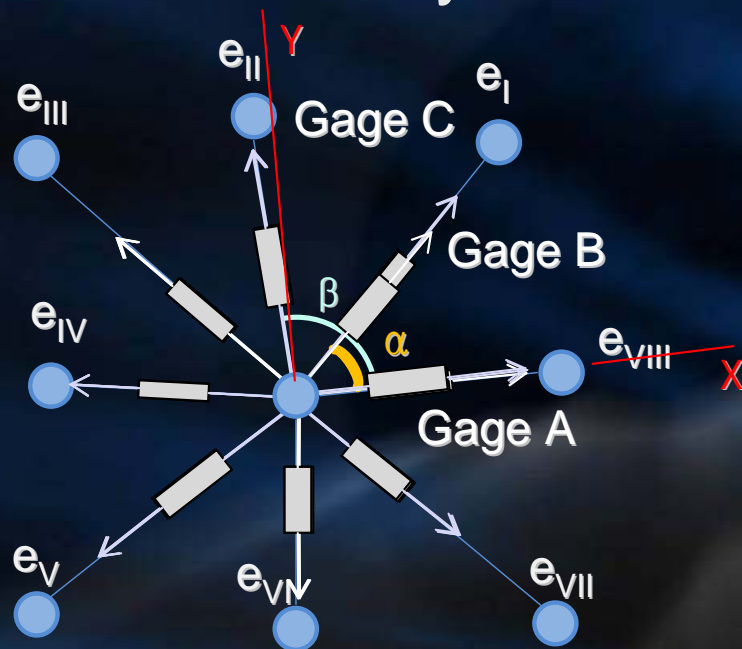
$$\varepsilon_b = \frac{\varepsilon_X + \varepsilon_Y}{2} + \frac{\varepsilon_X - \varepsilon_Y}{2} \cos 2\beta + \gamma_{XY} \sin 2\beta$$

$$\varepsilon_c = \frac{\varepsilon_X + \varepsilon_Y}{2} + \frac{\varepsilon_X - \varepsilon_Y}{2} \cos 2\gamma + \gamma_{XY} \sin 2\gamma$$



Analysis of deforming surface

➤ Local strain analysis on deforming mesh surface



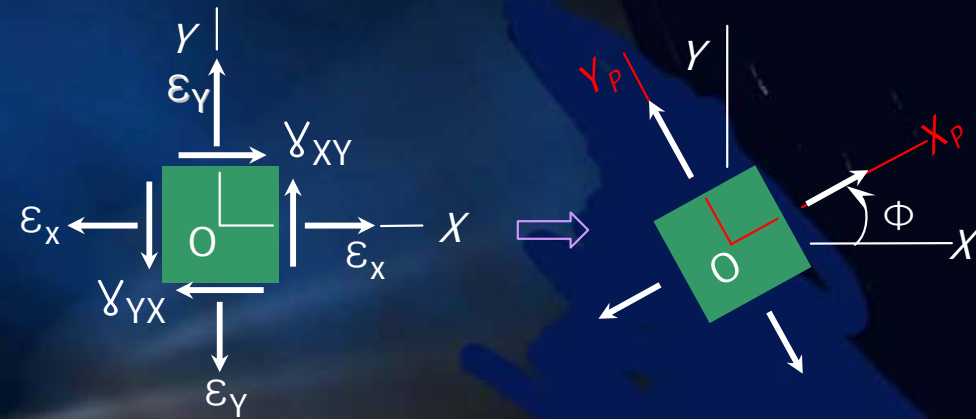
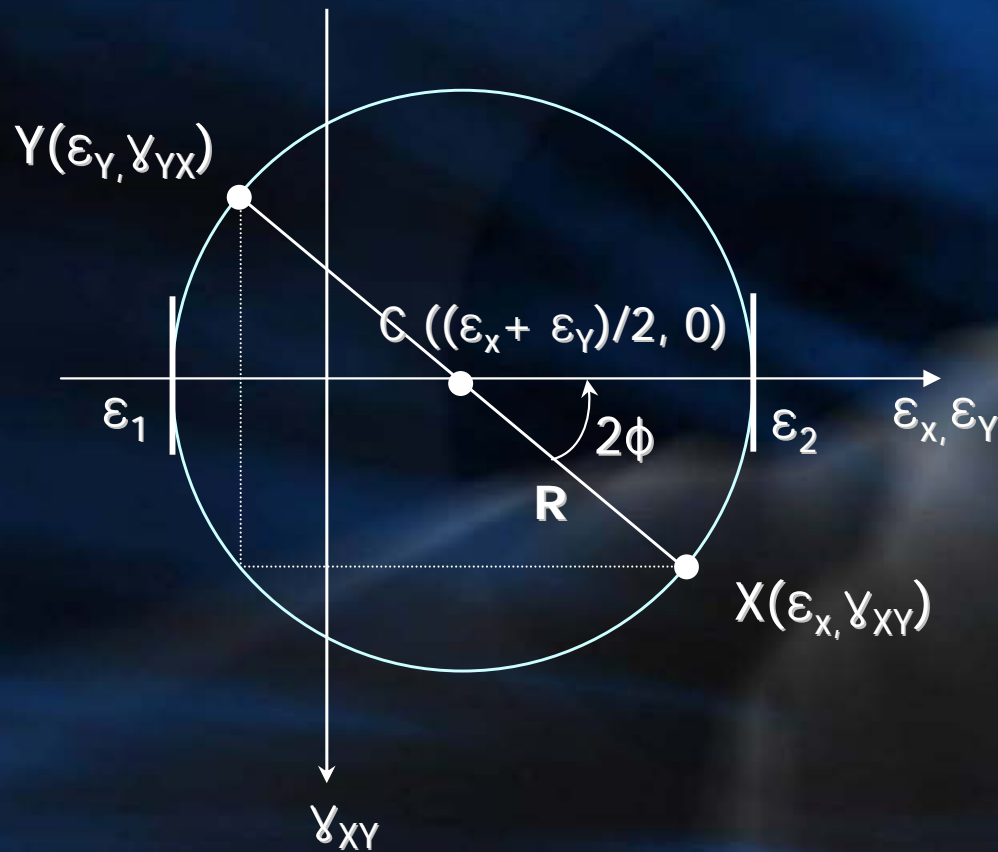
$$\varepsilon_A = \frac{\varepsilon_X + \varepsilon_Y}{2} + \frac{\varepsilon_X - \varepsilon_Y}{2} \cos(2 \times 0) + \frac{\gamma_{XY}}{2} \sin(2 \times 0)$$

$$\varepsilon_B = \frac{\varepsilon_X + \varepsilon_Y}{2} + \frac{\varepsilon_X - \varepsilon_Y}{2} \cos(2 \times \alpha) + \frac{\gamma_{XY}}{2} \sin(2 \times \alpha)$$

$$\varepsilon_C = \frac{\varepsilon_X + \varepsilon_Y}{2} + \frac{\varepsilon_X - \varepsilon_Y}{2} \cos(2 \times \beta) + \frac{\gamma_{XY}}{2} \sin(2 \times \beta)$$

- Use measured values $\varepsilon_A, \varepsilon_B, \varepsilon_C$ and compute $\varepsilon_x, \varepsilon_y, \gamma_{xy}$
normal strain shear strain
- Compute principal strains using Mohr's circle
- Average all principal strains

Mohr's circle for strain element



$$R = \frac{1}{2} \sqrt{(2\gamma_{xy})^2 + (\epsilon_x - \epsilon_y)^2}$$

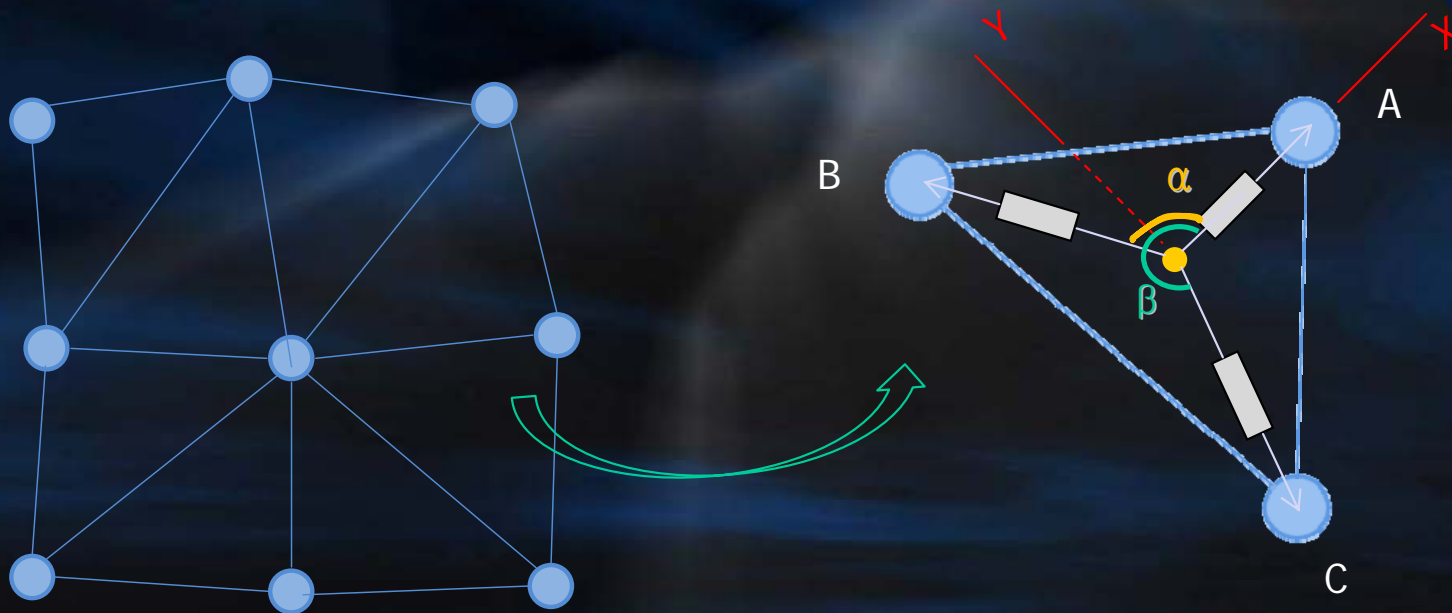
$$\epsilon_1 = \frac{\epsilon_x + \epsilon_y}{2} - R \quad \epsilon_2 = \frac{\epsilon_x + \epsilon_y}{2} + R$$

$$\Phi = \frac{1}{2} \tan^{-1} \left(\frac{\gamma_{xy}}{\epsilon_x - \epsilon_y} \right)$$

$\epsilon_x, \epsilon_y, \gamma_{xy} \Rightarrow$ compute principal strain values ϵ_1, ϵ_2 , and directions ϕ

Problems

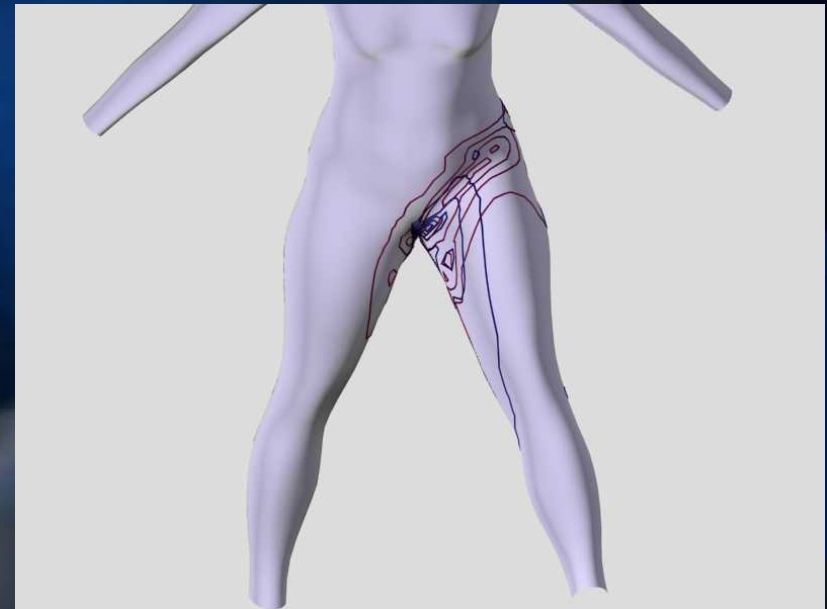
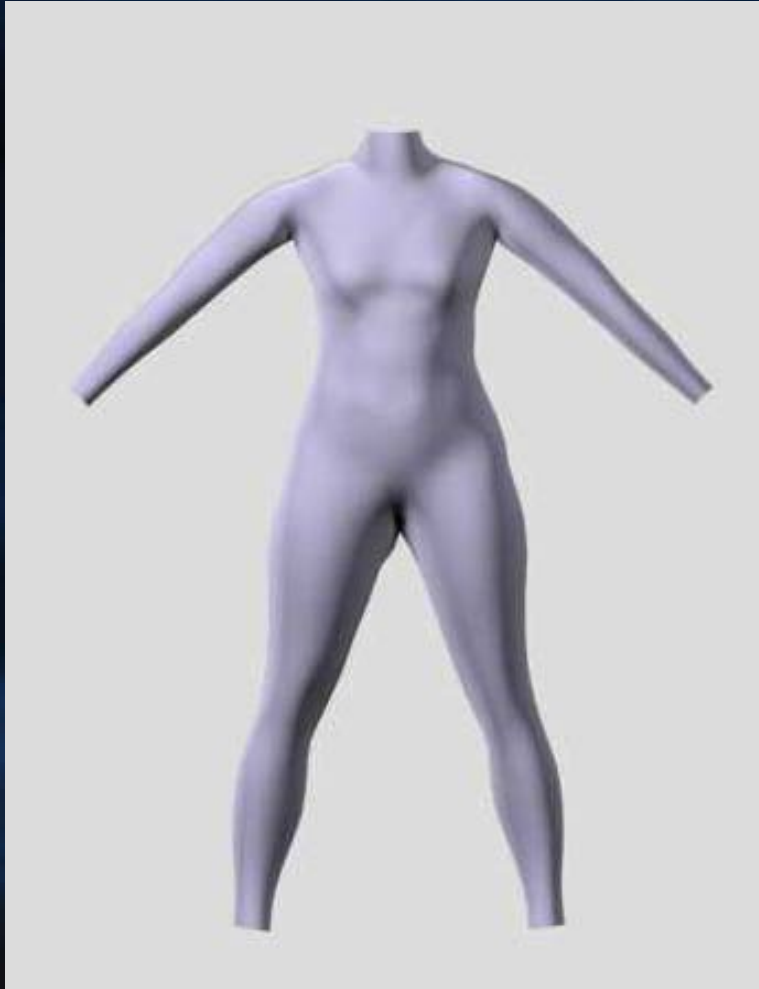
- Principal directions NOT tangential to the surface!!
- Solution: virtual strain gage on triangles



Results on a deforming mesh

- Maximum strain directions and values
 - Maximum strain values on bending knees
 - Maximum strain values on raising legs
 - Maximum strain directions on bending knees

Isocurves based on the maximum strain



Potential application

➤ Langer's lines

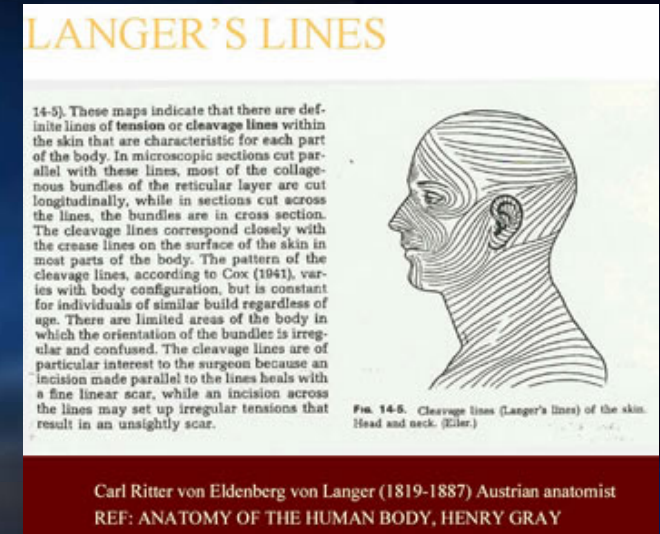
➤ After an Austrian anatomist Karl Langer

- ✓ first discovered by a French surgeon Baron Dupuytren

➤ Predominant alignment of collagen fibers within the dermis

➤ Important for surgical operation

- ✓ Incisions made parallel to Langer's lines may heal better and produce less scarring



Conclusion

➤ Registration

➤ New objectives

- Registration using dynamic features
- Overall framework

➤ On-going work on

- Data acquisition
- Data analysis
 - ✓ Local strain analysis adopting virtual strain gage
 - ✓ Extracted features: principal strain values and directions
- Results

Acknowledgment

- Prof. M. de Mathelin and Dr. P. Germain
 - Introduction and access to tagged MRI data